

**FINAL
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SUMMARY**

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The NANOCI project may help to improve auditory resolution at decreased energy consumption in future cochlear implants, world-wide used prostheses to restore hearing in the deaf. Proof of concept was obtained for guided growth of auditory neurons towards the stimulating electrodes *in vivo* and for an up to five-fold reduction of energy needed for stimulation *in vitro*, thereby offering a solution to improve the man:machine interface in the inner ear.

Functional hearing can be restored in the majority of deaf patients today using a neuro-prosthesis called cochlear implant (CI, Figure 1). Over 300,000 of these devices are currently in use worldwide and allow the majority of deaf-born children and deafened adults to use the sense of hearing to a degree that spoken language can be understood, thereby enabling oral communication.

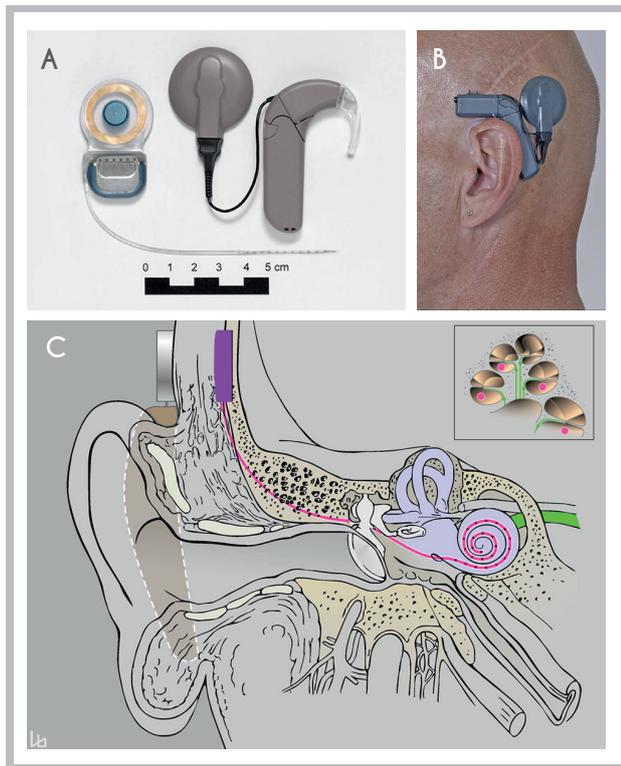
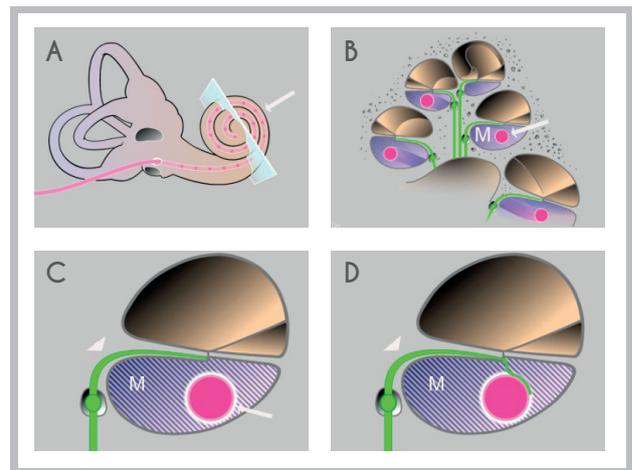


Figure 1. ▲ MED-EL cochlear implant system with implantable stimulator/receiver unit and externally worn speech processor (A). Clinical CI system with behind-the-ear speech processor (B). Schematic view with CI electrode array (pink) inserted into the cochlea of the inner ear for direct stimulation of the auditory neurons (green, C).

Despite the success, some limitations remain, which are mainly caused by the anatomical gap between auditory neurons and the electrode array in the cochlea. NANOCI aimed at improving CI performance by creating a gapless man:machine interface in the inner ear (Figure 2). Methods of biomedical engineering, regenerative medicine and nanotechnology have been used in concert to achieve the ambitious goal defined at the beginning of the project.



Proof of concept for guided growth of auditory neurons *in vivo*

Brain-derived neurotrophic factor (BDNF), tetrahydroflavone (THF) or a small protein mimetic of BDNF (L2) were chronically released over 4 weeks in the cochlea of deafened guinea pigs from reservoirs on the animal-grade *nanoCI* electrode and from the *nanoCI* gel-matrix in the scala tympani. In response to this treatment, auditory neurons in BDNF and THF treated deaf animals were guided through the nanomatrix-filled scala tympani towards the neurotrophin source on the electrode array (Figure 3). In most of the cases, the auditory neurons took a sharp turn immediately before the organ of Corti region (Figure 3A) growing downward and

Figure 2. ▲ The main aim of the NANOCI project is to eliminate the anatomical gap between the intracochlear electrode array (arrow in Figs. A-D) and the peripheral processes of the auditory neurons (arrowheads in Figs. C, D). The nerves will be attracted through surface release of growth factors from the array (arrow in Fig. C), supported and guided through the scala tympani using a neurotrophic nanomatrix (M) and permanently locked on the array through nanostructuring of the surface (D).

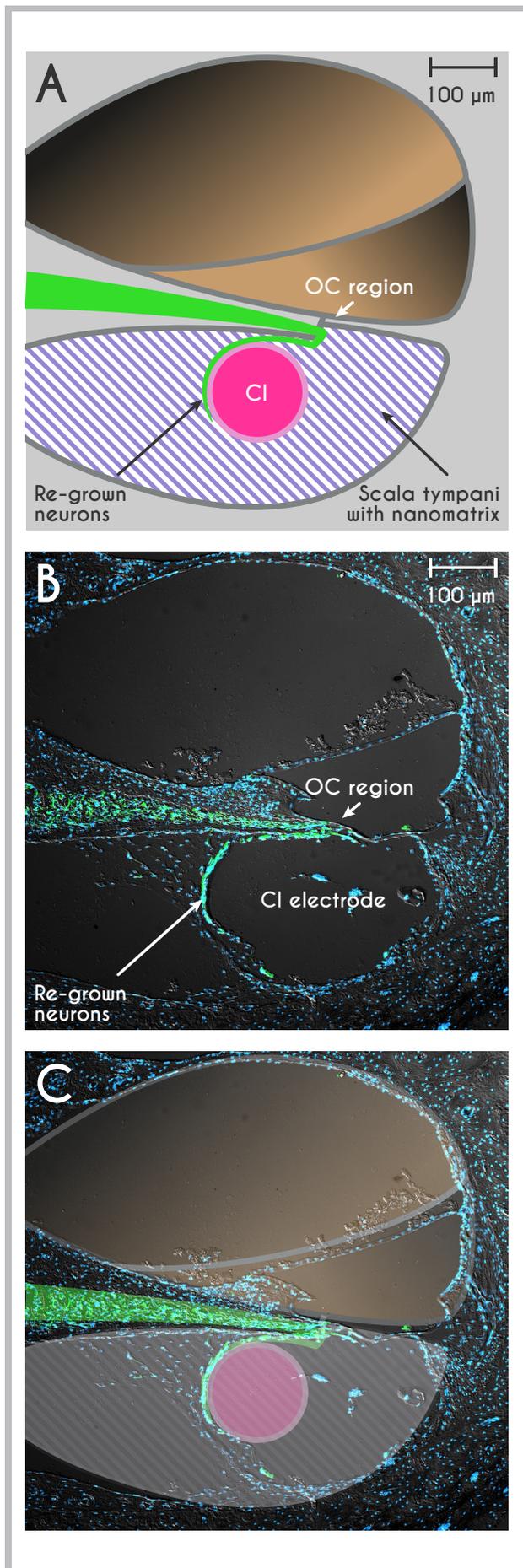


Figure 3. Guided growth of auditory neuronal fibers (green) from the organ of Corti (OC) region towards the drug-releasing nanomatrix (blue-shaded area) and cochlear implant electrode array (CI, pink) to form a gapless neuron:electrode interface in concept (A), *in vivo* (B) and merged (A+B = C). The electrode materials (silicone and platinum) are difficult to section and visualize, however the space occupied by the CI electrode is well delineated (B). The CI electrode implanted was larger compared to the original concept (difference of CI electrode area in C).

along the border of the *nanoCI* electrode array to form a gapless neuron:electrode interface (Figure 3B), very close as foreseen in the original concept of the project (Figures 3C).

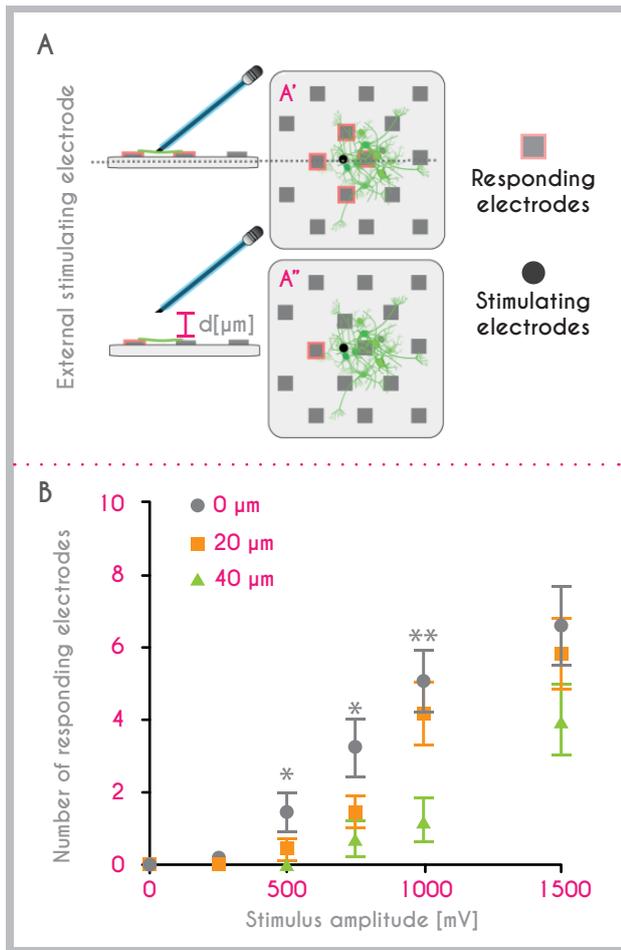
The gapless neuron:electrode interface opens the door for energy-efficient stimulation

Objective hearing tests showed some small improvements in hearing thresholds and amplitudes in deafened animals implanted with *nanoCI* gel-matrix and a combination of gel-matrix and *nanoCI* electrode array (as shown in Figure 3) compared to deafened control animals *in vivo*. However, these differences did not reach statistical significance, mostly due to the small numbers of animals tested in each group. The clear trend to improved functional results was corroborated instead by highly significant advantages of the gapless neuron:electrode interface in the *in vitro* setup, where response profiles of murine and human auditory neurons were obtained on multi-electrode arrays (Figure 4).

By modifying stimulus parameters in the gapless position on the multi-electrode arrays, an up to four-fold reduction of energy needed to elicit a response was observed (Figure 5).

Other significant achievements

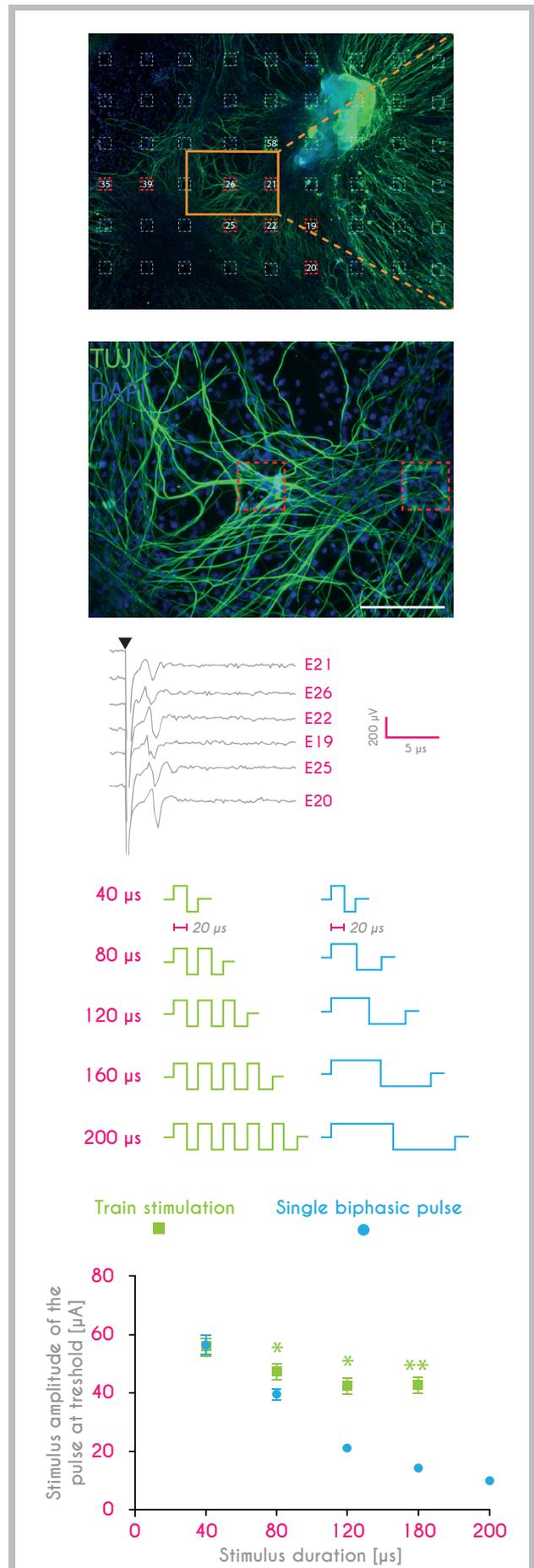
Novel bioactive compounds have been developed and tested for their capacity to stimulate neurite outgrowth. Most notably, a lead structure of a small-peptide mimetic of BDNF has been identified, which is ready for patenting. The functionalized *nanoCI* gel-matrix (Figure 2 “M” and Figure 3) containing laminin epitopes was successfully applied *in vivo*. New nanoparticles have been developed with antibacterial activity at reduced toxicity for coatings of the



electrode array. Other nanomaterials have been produced for functional modifications to optimize electrode conductivity, reduce impedance and improve neuron-electrode coupling in the scenario of the gapless interface. It is important to mention that all nanomaterials produced during the project have been tested for toxicity in appropriate and validated bioassays. Dispenser technologies have been investigated in order to obtain growth-factor/neurotrophin release from the CI electrode surface. Methods to visualize this neurotrophin-re-

Figure 4. ▲ Murine auditory neurons were cultured on multi-electrode arrays (MEAs) and stimulated from an externally mounted cochlear implant electrode array at various distances, ranging from 40 μm to 0 μm (A). In the gapless position (0 μm), more electrodes responded, enabling the reduction the stimulus amplitude and thereby also the minimal energy needed to elicit a response (B). We calculated a five-fold energy reduction when stimulating in the gapless position compared to a distance of 40 μm (1.5 nJ vs. 7.5 nJ).

Figure 5. ► Auditory neurons (immunostained for the neuronal marker TUJ) on MEAs (68 electrodes 40x40 μm^2) and representative traces of responding electrodes after electrical-induced response (upper panels). An example of the pulse shapes tested (lower middle graph) and corresponding threshold values to elicit response (bottom graph).



will remain active for another 5 years beyond the end of the official project duration.

Exploitation

A total of 4 patents to protect intellectual property related to NANOCI have been filed or are in preparation at the end of the project. In addition, over a dozen individual exploitation tracks have been identified, which will be pursued beyond the NANOCI project. These exploitation tracks include further developments of neurotrophin biomimetic molecules, nano-matrix gels, conductive and antibiotic nanoparticles, optic sensors, mathematical neuron models, *in vitro* and *in vivo* bioassays (as shown in Figures 3, 4 and 5), controlled drug-release and medical imaging technologies (as shown in Figure 6), among others.

Potential impact of the NANOCI project

Combining all developments of the NANOCI project, the proof of concept for the gapless interface between auditory neurons and the cochlear implant electrodes has been obtained *in vivo* (Figure 3). The *in vitro* setup confirmed the hypothesis that a significant reduction in energy used to stimulate the auditory neurons can be achieved, notably a five-fold reduction for the gapless position and a four-fold reduction, if stimulus parameters are optimized for the new interface (Figures 4 and 5). Together, these key findings lay the foundation to develop cochlear implant systems in the future with more specific and more energy-efficient stimulation of auditory neurons. Whereas the higher specificity of stimulation may result in better auditory resolution and improved hearing performance in music or background noise, the reduced energy consumption may be the key to develop smaller and more cost-efficient cochlear implants. If only a part of the energy-reduction obtained in the *in vitro* setup can be carried over to a clinical-grade cochlear implant system in the future, this may help to develop fully implantable devices, which would make hearing loss invisible, thereby increasing the acceptance by hearing impaired patients.

The other achievements of the project offer additional opportunities for researchers and SMEs in Europe. Of particular interest are the lead structures for BDNF – biomimetics and antibiotic nanoparticles, which may be worth the whole project's investment, in case they can be carried over into the world-wide market.

Overall, NANOCI was to our own judgment a successful project yielding new evidence on many different topics and bringing together scientific groups and SMEs from a variety of backgrounds. We would like to express our gratitude to the Seventh Framework Programme of the EU for the support of this exciting endeavor.

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